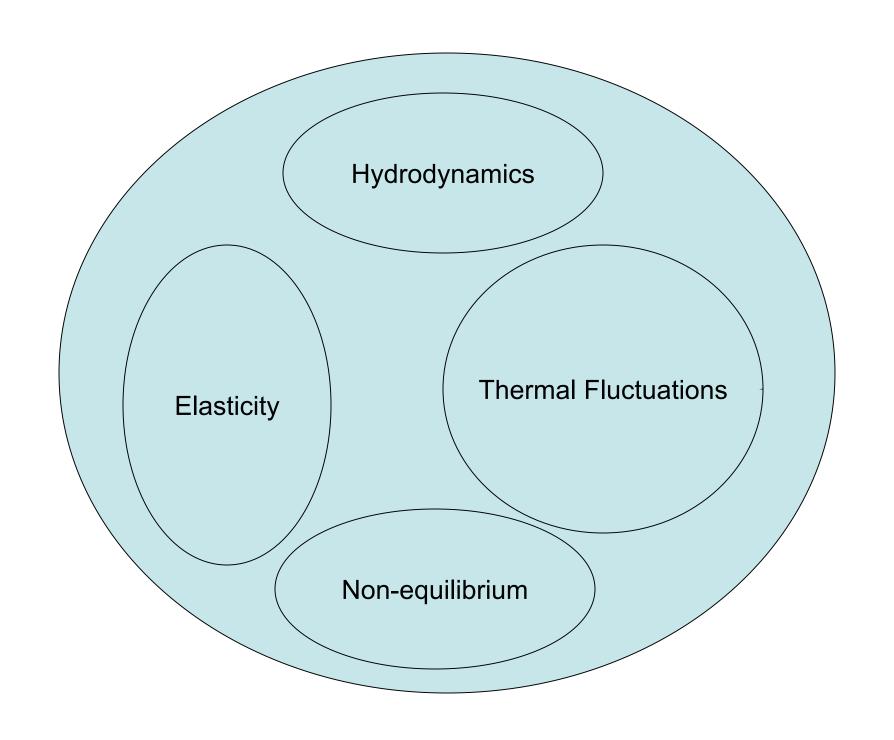
Propulsion with stiff polymers

Manoel Manghi (Toulouse)
Yong-Woon Kim (UCSB)
X. Schlagberger, Roland Netz (TUM)

PRL 96, 068101 (2006) PRL in press (2006)

- 1) sedimentation of polymers
- 2) electrophoresis of polymers
- 3) polymers in shear flow (unfolding of proteins in blood flow)
- 4) polymers at surfaces in shear or electric fields (glycocalix deformation under shear)
- 5) driven stiff polymers -> propulsion



Hydrodynamics at low Reynolds numbers

Stationary Navier-Stokes equation
$$\eta \, \Delta \vec{v}(\vec{r}) - \nabla p = \rho(\vec{v}, \nabla) \vec{v}$$

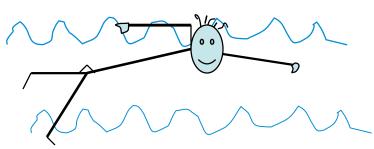
If the Reynolds number
$$Re^{tr}=rac{
ho}{\eta}\,l\,v\ll 1$$
 , $Re^{rot}=rac{
ho}{\eta}\,r^2\,\omega\ll 1$,

one obtains the **creeping flow equation.**

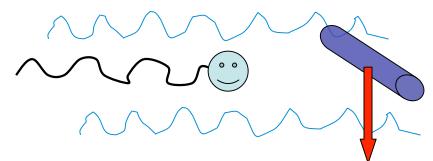
human

<u>bacterium</u>

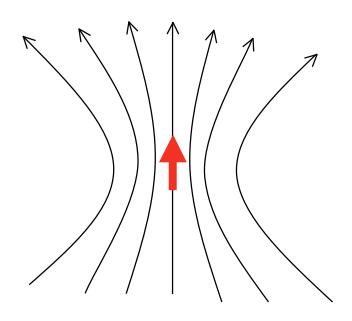
sinking cylinder



$$\begin{array}{c} H_2O: \ \eta = 0.001 \ Pa \ s; \\ \rho = 1000 \ kg/m^3 \\ v = 1 \ m/s \\ 1 = 1 \ m \end{array} \begin{array}{c} v = 10^{-5} \ m/s \\ 1 = 1 \ \mu \\ \rightarrow \ Re = 10^{-7} \end{array} \begin{array}{c} v \sim 10^{-7} \ m/s \\ 1 = 1 \ \mu \\ \rightarrow \ Re = 10^{-7} \end{array}$$



$$v = 10^{-5} \text{ m/s}$$
 $v \sim 10^{-7} \text{ m/s}$
 $1 = 1 \mu$ $1 = 1 \mu$
 $\Rightarrow \text{Re} = 10^{-5}$ $\Rightarrow \text{Re} = 10^{-7}$

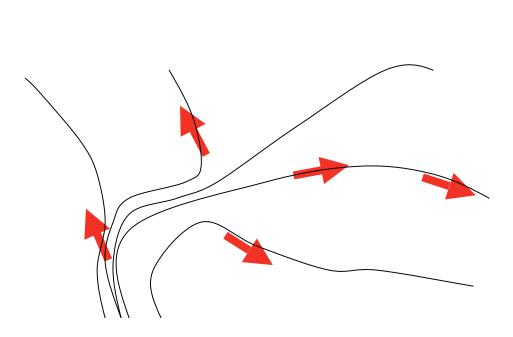


flow-field due to point-force at origin:

$$u^{\alpha}(r) = H^{\alpha\beta}(r) f^{\beta} \qquad \alpha, \beta = 1, 2, 3$$

$$H^{\alpha\beta}(r) = \frac{1}{8\pi\eta r} \left[\delta_{\alpha\beta} + \hat{r}^{\alpha} \hat{r}^{\beta} \right]$$
(Oseen-Tensor)

for many particles the superposition principle is valid:



$$u^{\alpha}(r) = \sum_{i} H^{\alpha\beta}(r - r_i) f_i^{\beta}$$

invert to get forces for prescribed solvent velocity distribution!!

Next: add thermal noise

Theoretical Framework: Position Langevin Equation

Velocity of i-th particle:
$$m\ddot{r}_j(t)\ddot{\mu}_{ij} + \dot{r}_i(t) = \ddot{\mu}_{ij} f_j(t) + \xi_i(t)$$

deterministic force
$$f_j(t) = -\partial U(t)/\partial r_j(t) + E$$

Random force
$$\langle \xi_i(t) \xi_j(t') \rangle = 6 \vec{\mu}_{ij} k_B T \delta(t-t')$$

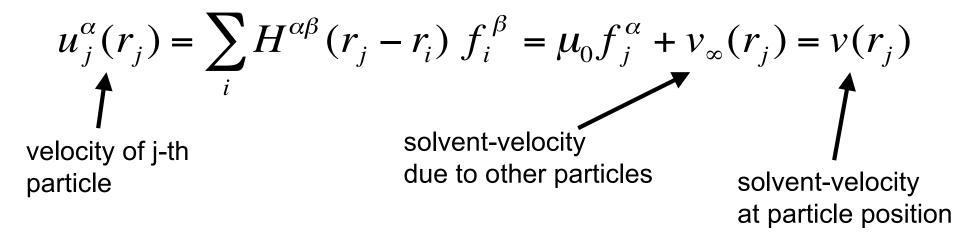
Mobility matrix:
$$\vec{\mu}_{ij} = D_{ij} / k_B T = \mu_0 \delta_{ij} + \vec{H}(r_i, r_j)$$

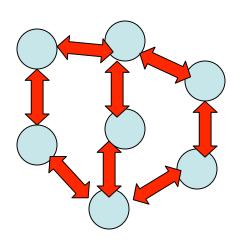
self mobility:
$$\mu_0 = (6\pi R \eta)^{-1}$$
 hydrodyn. interact.

equivalent to Smoluchowski equation for particle distribut. W(r_i,t):

$$\frac{\partial W}{\partial t} = \sum_{i,j} \frac{\partial}{\partial r_i} \left[D_{ij} \frac{\partial W}{\partial r_j} - \mu_{ij} f_j W \right] \quad \text{with solution:} \quad W \cong e^{-U/k_B T}$$

straightforward way to satisfy no-slip in multi-particle system

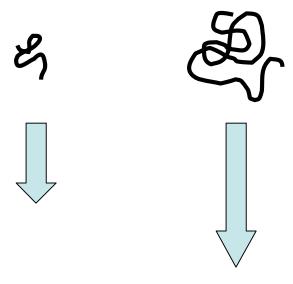




cohesive/elastic forces in objects automatically lead to solvent flow stagnation

a few examples

Separation by sedimentation in the ultracentrifuge



G: force per monomer

N: monomer number

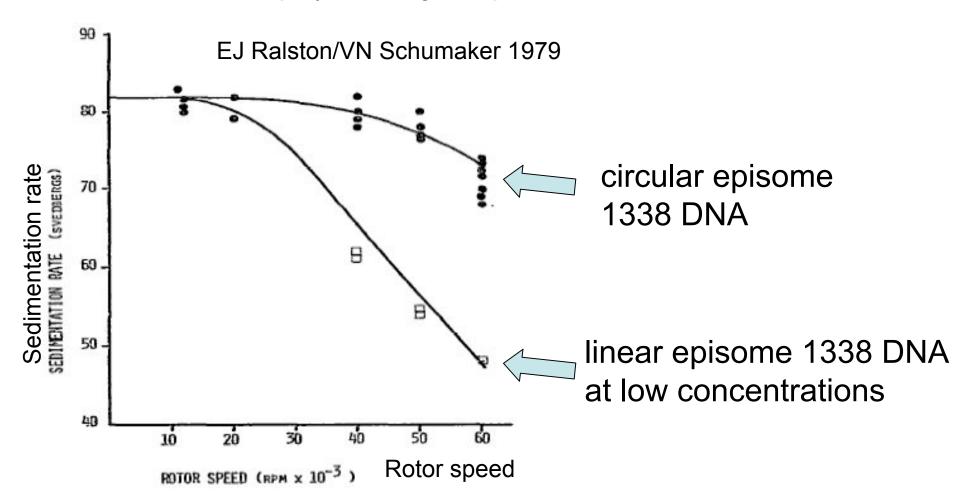
velocity v= $GN\mu$

mobility $\mu=1/6\pi\eta R=1/6\pi\eta N^{\nu}$

--> velocity $v \approx G N^{1-v}$

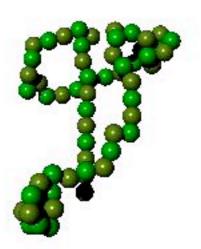
Why gel-electrophoresis is used for separating DNA (and not the ultracentrifuge)

- sedimentation rate of polymers goes down at high rotor speeds
- crossover is polymer-length dependent!



Crumpling of Flexible Chains (Xaver Schlagberger)





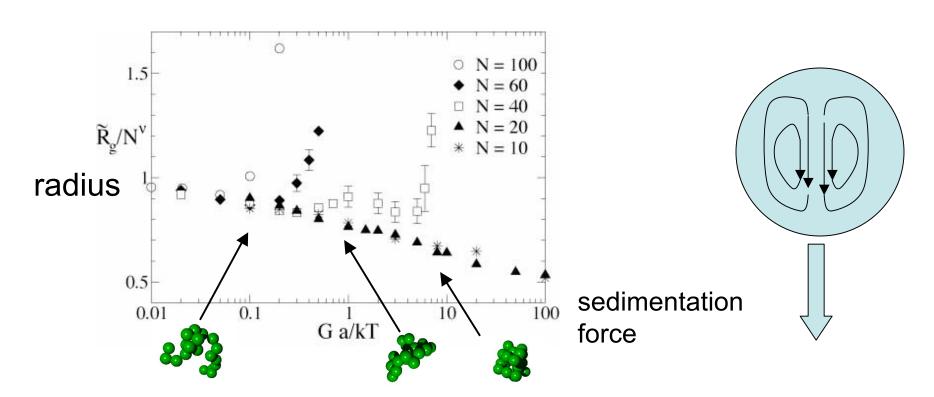
hydrodynamic simulations of sedimenting polymers

Xaver Schlagberger

hydrodynamic drag -> internal recirculation with velocity $v \approx GN/\eta R$ -> recirculation time scale $\tau_{flow} \approx R/v \approx \eta R^2/GN$

compare with coil relaxation time $\tau_R \approx \eta R^3 / k_B T$

,,scrambled/collapsed coil" for $\tau_R > \tau_{flow}$ or Ga/k_BT > N^{-2/3}



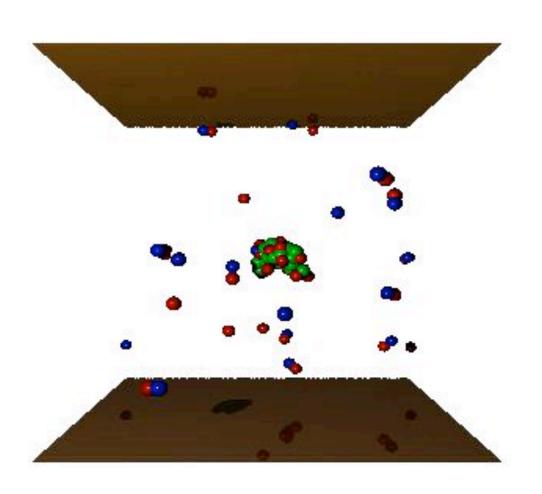
Sedimentation of twisted ring polymer (conserved linking number) Hirofumi Wada



Dynamics of plectoneme formation in ring polymer Hirofumi Wada



Electrophoresis of polyelectrolytes



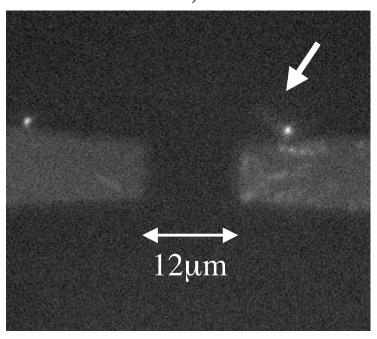
20 monomers40 counterions20 coions

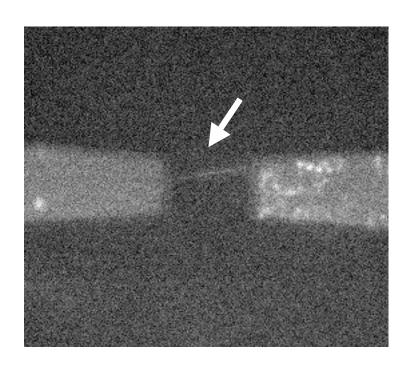
electric field, camera moves with polymer!

minimal image BC strong coupling $\Xi = 20$

experimental observation of DNA stretching in fields Beyer, Simmel (LMU)

4 Volts -> E = $3 \times 10^5 \text{ V/m}$ DNA length $17\mu\text{m}$ 10mM HEPES, no added salt





DNA-molecules are typically stretched in free-solution electrophoresis experiments -> no length separation possible

Protein denaturation in shear flows

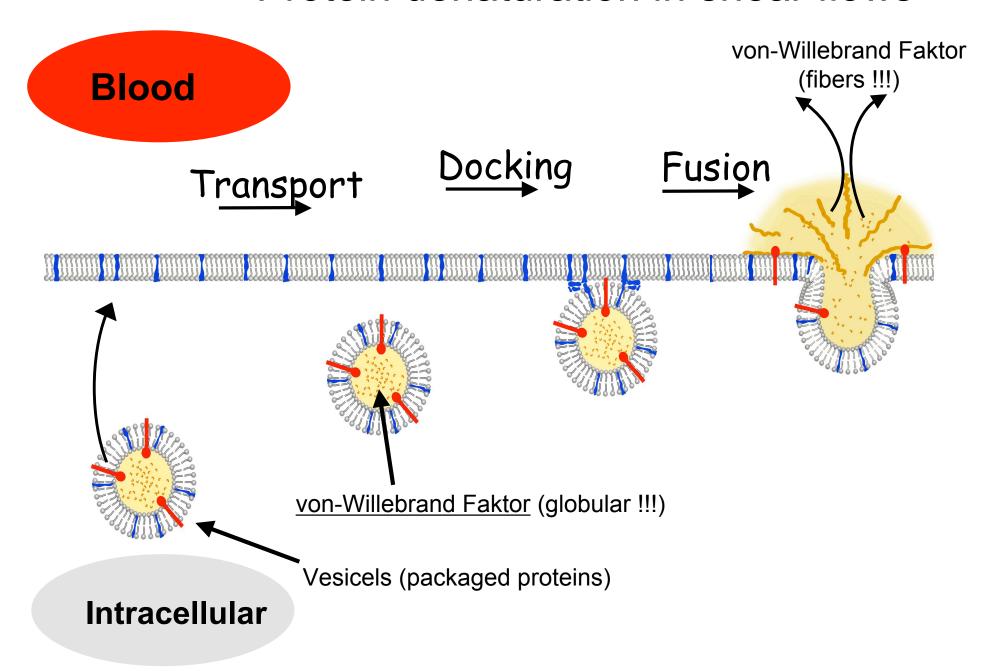
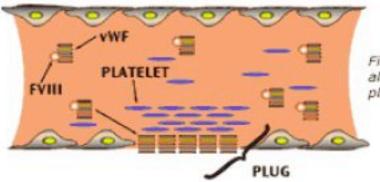


Figure 1. Normal Broken Blood Vessel



First, vWF proteins from the blood line up along the broken vessel wall and attract "sticky" platelets to form a plug.

Then the platelets attract strands of fibrin to strengthen the plug and form a clot. The clot helps stop the bleeding.

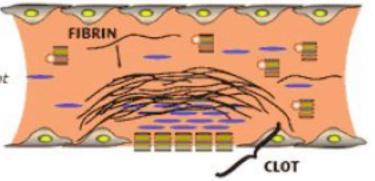
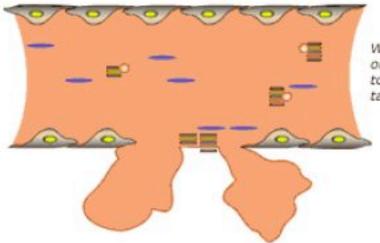


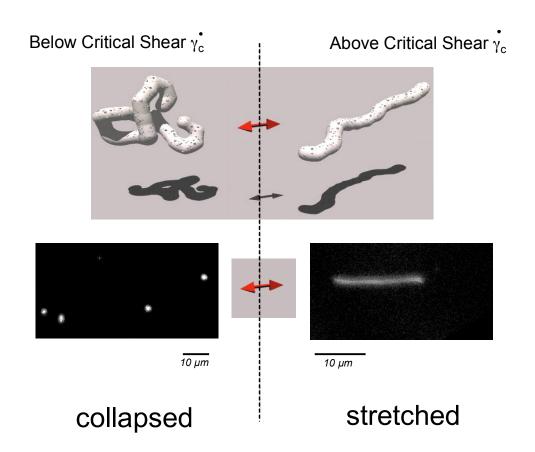
Figure 2. Broken Blood Vessel in vWD

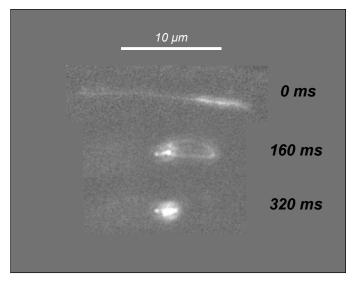


When a person has vWD, there isn't enough vWF or the vWF is damaged. The clot may take longer to form or not form properly, and bleeding make take longer to stop.

unfolding occurs also in bulk (without collagen substrate)

Schneider/Wixforth (Augsburg)

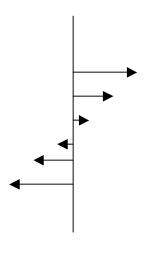


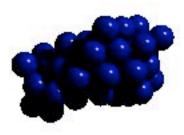


relaxation into globular state once shear is turned off

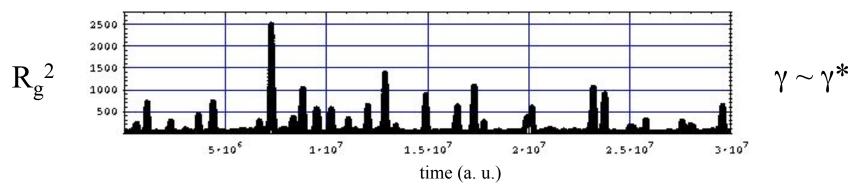
in shear, $\varepsilon=2.5$, $\gamma=1.2$

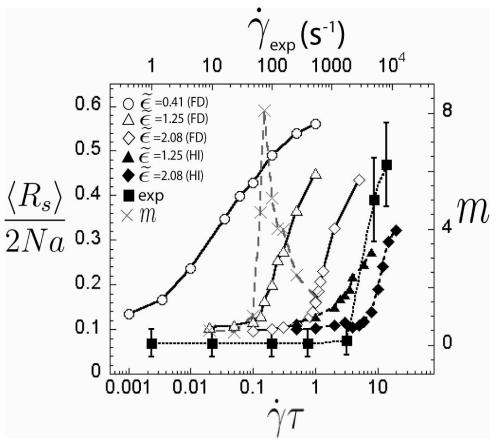
Alfredo Alexander-Katz





stretching dynamics





stretching response

unfolding becomes abrupt for globular proteins (in agreement with experiments)

Propulsion with Propulsion Propulsion Propulsion Stiff Polymers Stiff Polymers

produce shear with beating polymers

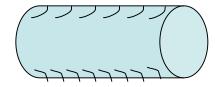
Ciliae

power stroke

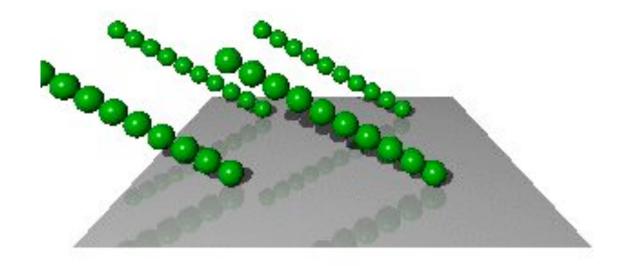
recovery stroke

propulsion

pumping



model polymer as isotropic elastic rod apply asymmetric torque at the polymer base -> measure net pumping velocity, efficiency, etc. Yong-Woon Kim, RRN



10

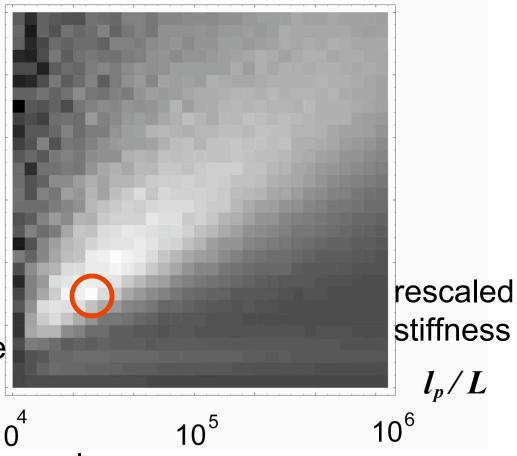
1. condition: threshold force for deformation:

$$\tau_f / k_B T \approx \ell_P / L$$

 τ_f/τ_b

ratio 4
forward torque/
backward torque

2. Condition: asymmetry

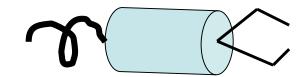


Symmetric motion: no net pumping

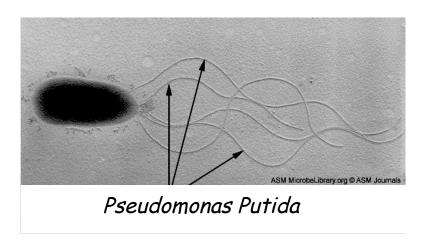
No elasticity: no net pumping (since reciprocal motion...)

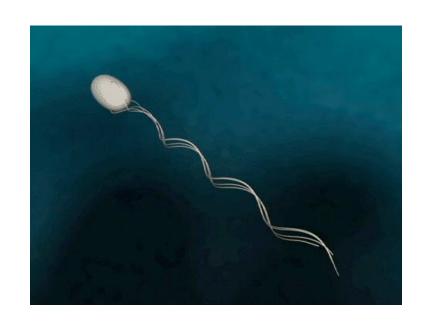
propulsion with single rotating polymers

goal: moving nanomachines



· Bacteria





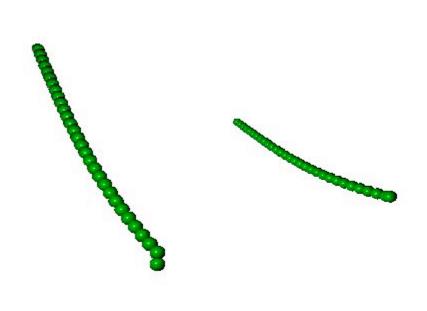
problem: - need helical polymer,

- rotational sense determines thrust direction

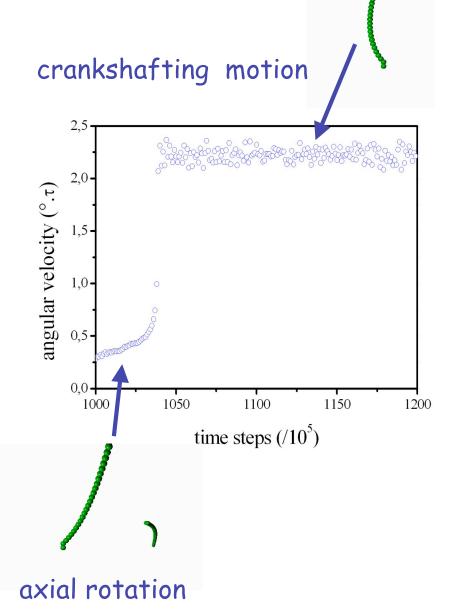
question: - propulsion possible with straight rotating polymers?

Dynamical transition for rotating straight flexible polymer

Manoel Manghi/ RRN

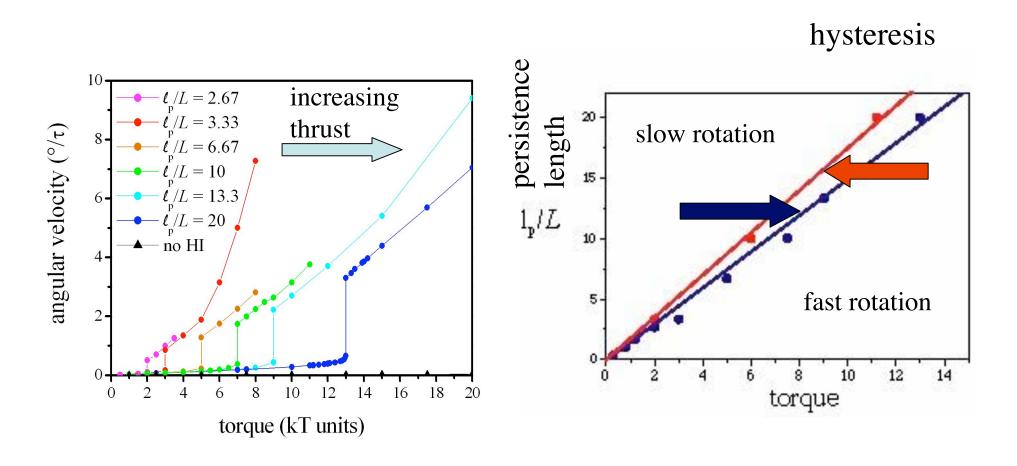


Torque =
$$4-5$$
 kT/rad ℓ_p = 6.7 L N = 30

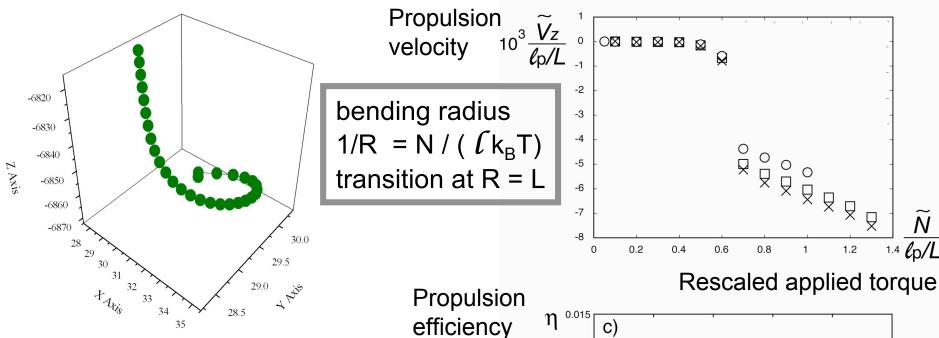


flexible polymer, l_P=L/3 effects of thermal fluctuations?

discontinuous non-eq. shape transition

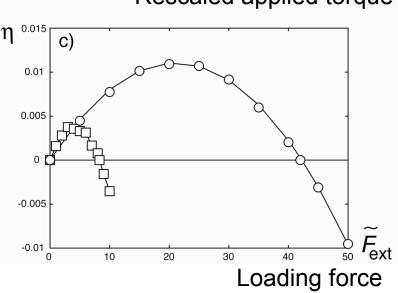


Propulsion due to breaking of time-reversal invariance of motion thrust direction independent of rotational sense!! ---> nano-force-rectifyer



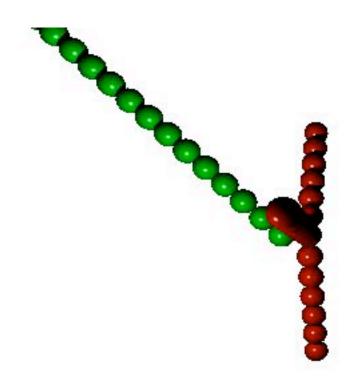
$$\eta = \frac{\text{propulsion power}}{\text{rotation power}}$$

efficiency low (but not worse than bacterial flagellae)



Flagellum with a base: total force and torque must be zero

- →rotation leads to counterrotation
- →trajectories are complex



Hirofumi Wada

first form helix (difficult!):

then rotate, slowly

quickly (periodic twist-stretch conversion)

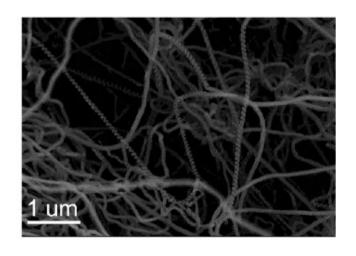
5



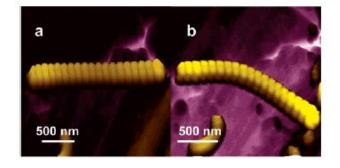
-shape (polymorphism??), bundling, efficiency.....

pulling on helical nanosprings

Hirofumi Wada (JSPS-fellow) & RRN

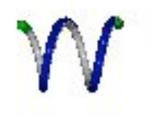


SEM characterization of as-synthesized silicon oxide nanowires

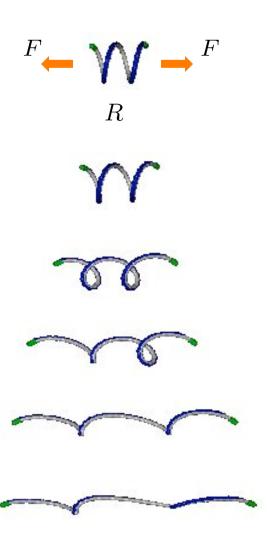


AFM manipulation of a helical silica nanospring

Hai-Feng Zhang et al. Nano Lett. 3 577 (2003)



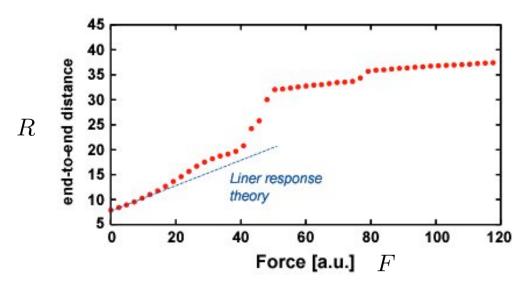
pulling on a nanospring



Linear response for small pulling force

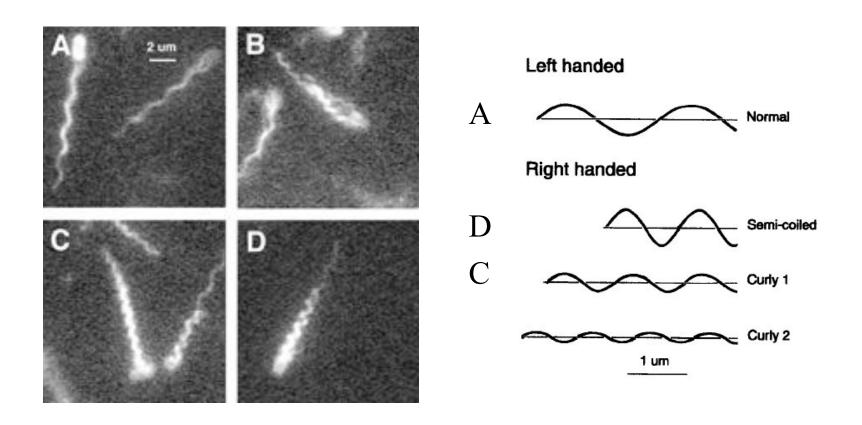
$$F \approx K_{sp}(R - R_0)$$

$$K_{sp} = \frac{\Omega_0^2}{L} \left[4A\beta^2 + C(1 - \beta^2)^2 \right]$$

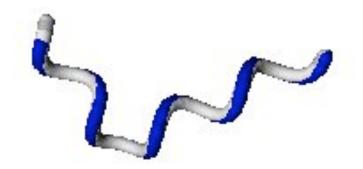


Force-extension curve reveals stretching instability of a helical nanospring.

Polymorphic transformations of flagellae as function of rotational sense and frequency



Dynamic conversion of bistable helix



design of simple propulsion devices with stiff polymers leads (naturally) to biomimetic structures